

# A Spatial Modeling Framework for Functional Neuroimaging Data

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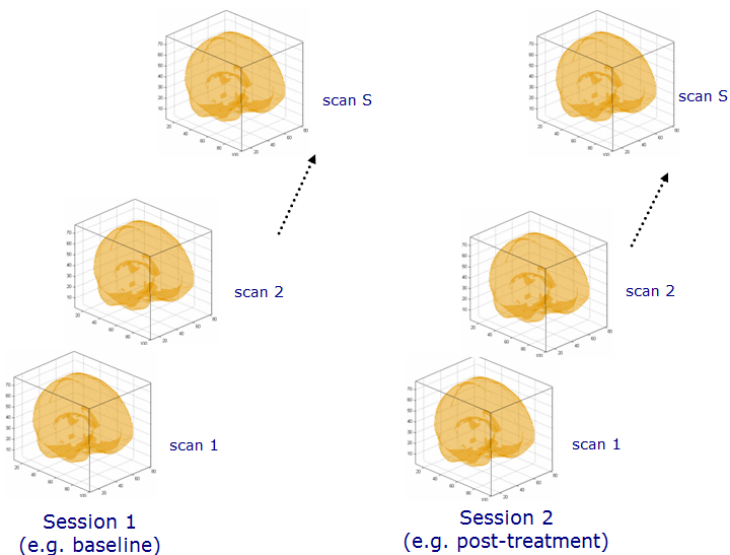
University of Florida Workshop on High Dimensional Inference



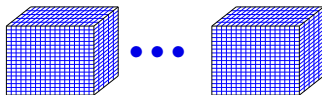
# Outline

- 1 Introduction
- 2 Spatial Modeling for Activation Studies
- 3 Spatial Prediction Model
- 4 Summary

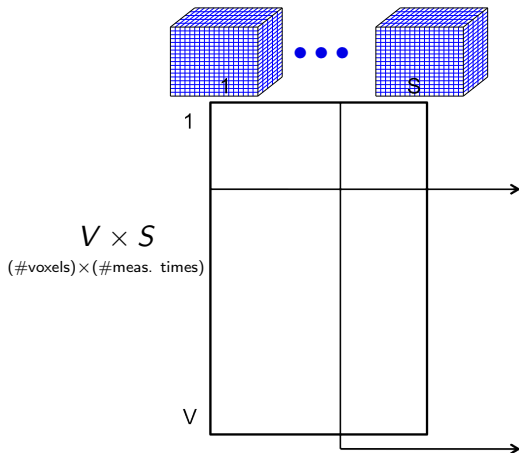
# Data Characteristics



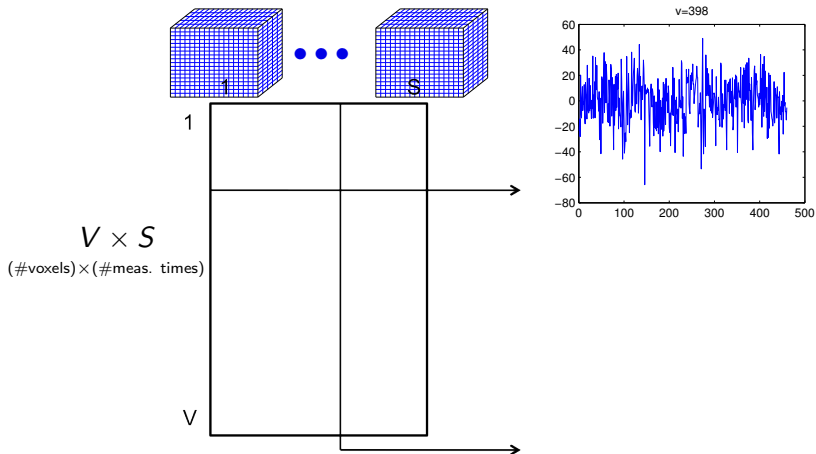
# Data Characteristics



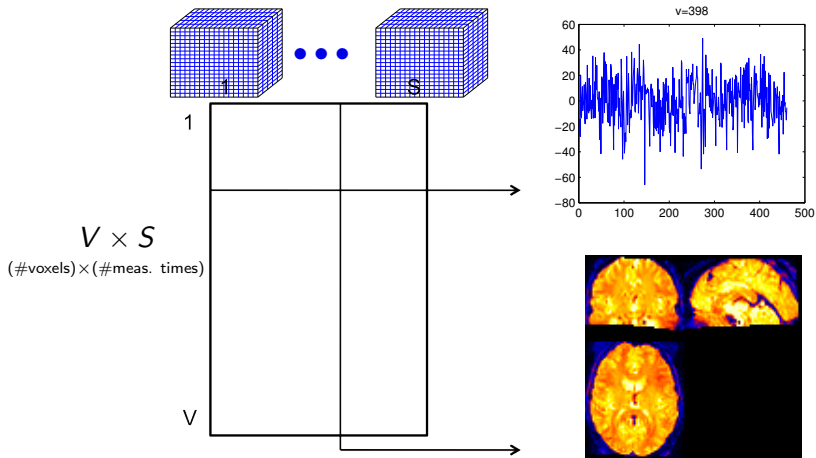
# Data Characteristics



# Data Characteristics



# Data Characteristics



# Data Example

## Working Memory in Schizophrenia Patients

- N=28 subjects: 15 schizophrenia patients and 13 healthy controls
- fMRI Tasks: Serial Item Recognition Paradigm (SIRP)
  - **Encoding set:** Subjects asked to memorize 1, 3, or 5 target digits.
  - **Probing set:** Subjects sequentially shown single digit probes and asked to press a button:
    - with their index finger, if the probe matched
    - with their middle finger, if not.
- 6 runs per subject: (177 scans per run for each subject)
  - 3 runs of working memory tasks on each of 2 days
- **Objective:** Compare working memory-related brain activity between patients and controls.

Data from the Biomedical Informatics Research Network (BIRN) [1]: Potkin et al. (2002), Proc. 41st Annu. Meeting Am.

College Neuropsychopharm.



# Data Characteristics

- Massive data sets

$N = 28$  subjects,  $V \approx 900,000$  voxels,  $S = 177$  scans per run, 3 runs each day, 2 days (sessions)

- Almost 1 billion spatio-temporal data points per subject! 26 billion for all subjects!!

- Temporal correlations

- Complex spatial correlations

# Common Neuroimaging Objectives



- 1 **Activation studies:** localize regions of the brain activity when performing an experimental task
- 2 **Connectivity studies:** identify what brain areas show similar patterns of activity over time  $\Rightarrow$  distributed networks of brain function
- 3 **Prediction studies:** use functional brain images to
  - predict neural activity
  - predict experimental conditions, behavior or a subject's group membership (e.g. psychiatric condition, treatment response)

# General Analysis Approach

- Fit a linear model separately for each subject (at each voxel)
  - Address correlations between scans using AR models (+ white noise)
    - Pre-coloring/temporal smoothing [Worsley and Friston, 1995]
    - Pre-whitening [Bullmore et al, 1996; Purdon and Weisskoff, 1998]
    - Alternative structures available for PET [Bowman and Kilts, 2003]
- Fit Stage II linear model that combines subject-specific estimates
  - A two-stage (random effects) model
    - Simplifies computations\*
    - Sacrifices efficiency
- Compute t-statistics at each voxel and threshold
  - Consider a multiple testing adjustment (Bonferonni-type, FDR, RFT)

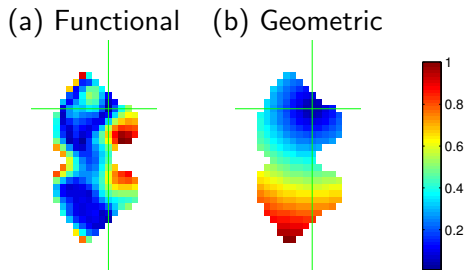
## Stage II Model Properties

- Voxel-by-voxel analyses
- Assumes independence between brain activity measures at different brain locations
- Targets activation analyses
- Disregards functional connectivity

# Spatial Correlations

## Distances

- Physical (**Geometric**)
- **Anatomical**
- **Functional**
  
- The complex neuroanatomy and neurophysiology make basic assumptions of many spatial methods questionable for neuroimaging

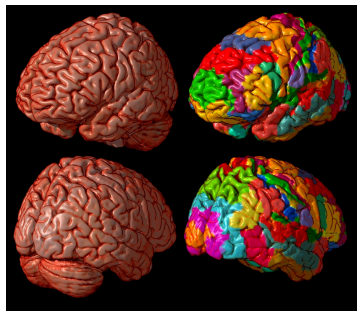


**Figure:** Selected axial slice of the cerebellum.

Bowman (2007), *JASA*.

# Spatial Modeling Framework

- **Stage I:** perform voxel-level GLM analyses for each individual (AR model for **temporal correlations**).
- **Stage II:** we propose models that address **spatial correlations**
  - Define brain regions using neuroanatomic parcellation (e.g. Brodmann or AAL)
  - **Spatial correlations**
    - Within regions
    - Between regions
  - Inferences
    - Voxel-level
    - Regional



## Stage II: Bayesian Spatial Model for Activation and Connectivity (BSMac):

$$\begin{aligned}
 \mathbf{Y}_{igj} \mid \boldsymbol{\mu}_{gj}, \alpha_{igj}, \sigma_{gj}^2 &\sim \text{Normal}(\boldsymbol{\mu}_{gj} + \mathbf{1}\alpha_{igj}, \sigma_{gj}^2 \mathbf{I}) \\
 \boldsymbol{\mu}_{gj} \mid \lambda_{gj}^2 &\sim \text{Normal}(\mathbf{1}\mu_{0gj}, \lambda_{gj}^2 \mathbf{I}) \\
 \sigma_{gj}^{-2} &\sim \text{Gamma}(a_0, b_0) \\
 \boldsymbol{\alpha}_{ij} \mid \boldsymbol{\Gamma}_j &\sim \text{Normal}(\mathbf{0}, \boldsymbol{\Gamma}_j) \\
 \lambda_{gj}^{-2} &\sim \text{Gamma}(c_0, d_0) \\
 \boldsymbol{\Gamma}_j^{-1} &\sim \text{Wishart} \{ (h_0 \mathbf{H}_{0j})^{-1}, h_0 \}
 \end{aligned}$$

- $\mathbf{Y}_{igj} = (Y_{igj1}, \dots, Y_{igjV_g})'$ ,  $\boldsymbol{\mu}_{gj} = (\mu_{gj1}, \dots, \mu_{gjV_g})'$ , and  $\boldsymbol{\alpha}_{ij} = (\alpha_{i1j}, \dots, \alpha_{iGj})'$

Bowman et al. (2008), *NeuroImage*

## BSMac

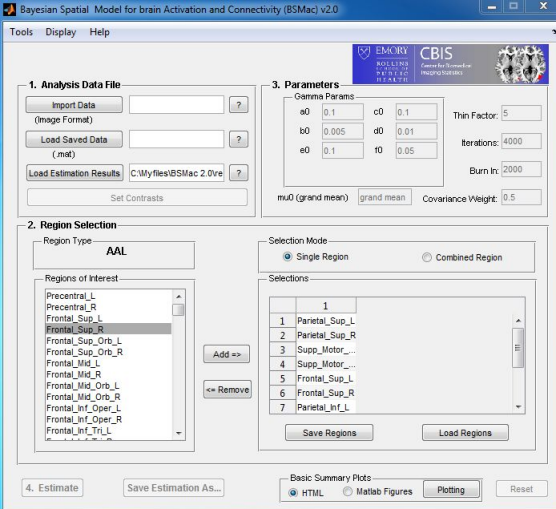


- MCMC via Gibbs Sampler
- Exchangeable correlation structure between voxels within the same brain region
- $\Gamma_j$  yields (unstructured) correlation model between regions
- Relatively fast estimation
- MATLAB Software available at [www.sph.emory.edu/bios/CBIS/](http://www.sph.emory.edu/bios/CBIS/)
- Related Spatial Models / Extensions: Derado et al. (2010), *Biometrics*
  - Extends model to capture temporal correlations between multiple scanning sessions (e.g. days or treatment periods)
  - BUT, does not capture between region spatial correlations



# BSMac MATLAB Toolbox

## GUI Interface



Bayesian Spatial Model for brain Activation and Connectivity (BSMac) v2.0

Tools Display Help

**1. Analysis Data File**

Import Data (Image Format) ?

Load Saved Data (.mat) ?

Load Estimation Results C:\Myfiles\BSMac 2.0\ve ?

Set Contrasts

**2. Region Selection**

Region Type: **AAL**

Regions of Interest:

- Precentral\_L
- Precentral\_R
- Frontal\_Sup\_L
- Frontal\_Sup\_R**
- Frontal\_Sup\_Orb\_L
- Frontal\_Sup\_Orb\_R
- Frontal\_Mid\_L
- Frontal\_Mid\_R
- Frontal\_Mid\_Orb\_L
- Frontal\_Mid\_Orb\_R
- Frontal\_Inf\_Oper\_L
- Frontal\_Inf\_Oper\_R
- Frontal\_Inf\_Tri\_L
- Frontal\_Inf\_Tri\_R

Add =>

<=< Remove

**3. Parameters**

Gamma Params

a0 0.1 c0 0.1

b0 0.005 d0 0.01

e0 0.1 f0 0.05

Thin Factor: 5

Iterations: 4000

Burn In: 2000

mu0 (grand mean) grand mean Covariance Weight: 0.5

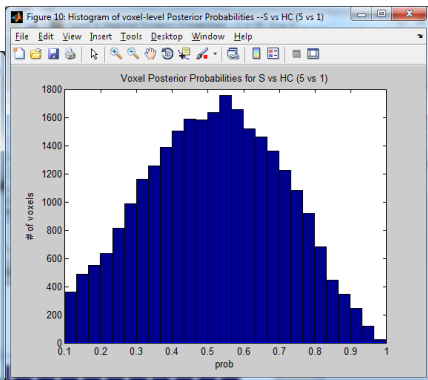
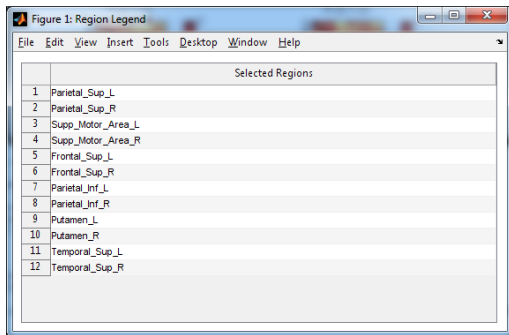
**4. Estimate** Save Estimation As...

Basic Summary Plots

HTML  Matlab Figures

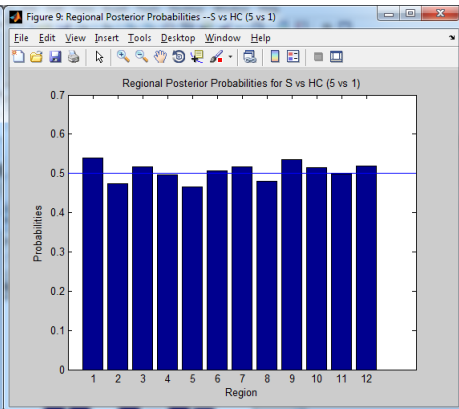
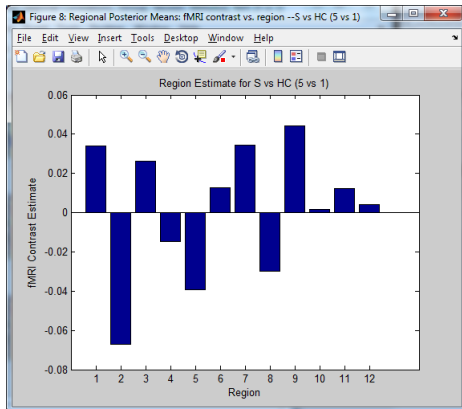
## BSMac MATLAB Toolbox

## Basic Summary Plots



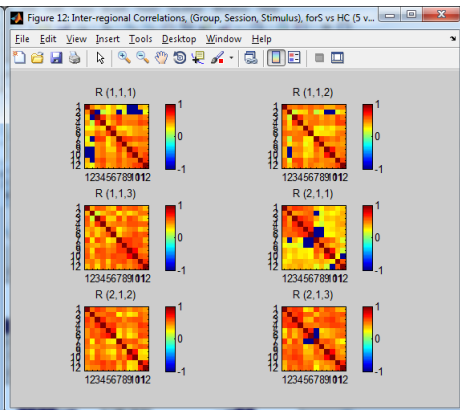
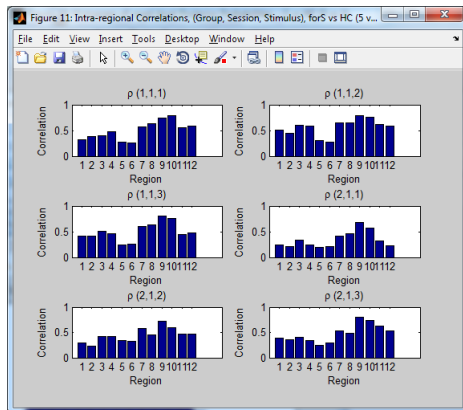
## BSMac MATLAB Toolbox

## Basic Summary Plots



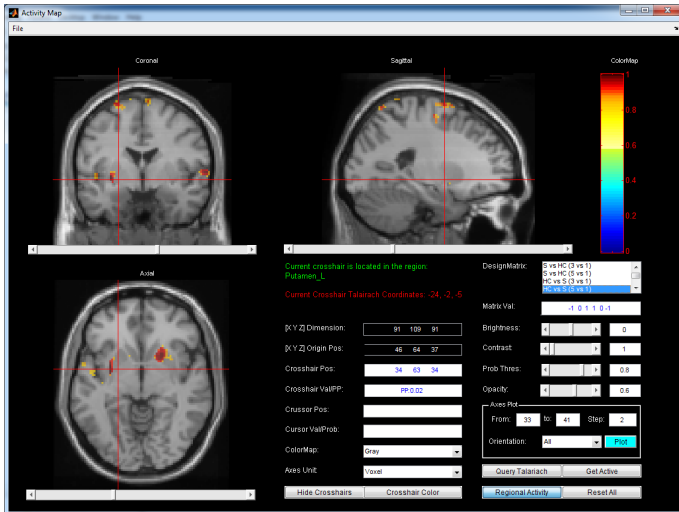
## BSMac MATLAB Toolbox

## Basic Summary Plots



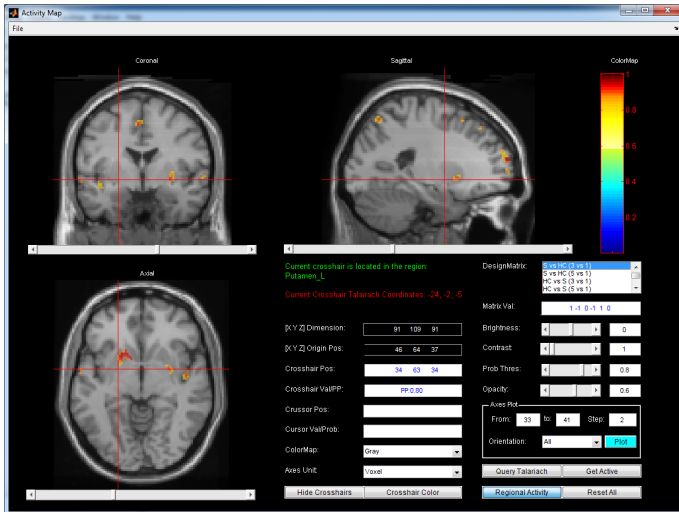
## BSMac MATLAB Toolbox

## Interactive Activation Maps



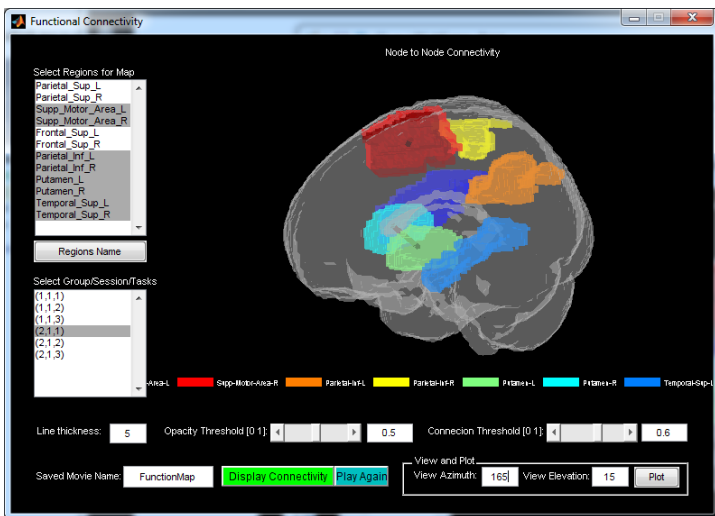
## BSMac MATLAB Toolbox

## Interactive Activation Maps



## BSMac MATLAB Toolbox

## Task-Related Connectivity Maps: Schizophrenia Patients



## BSMac MATLAB Toolbox

## Task-Related Connectivity Maps: Healthy Controls





# Conclusions: BSMac

## BSMac framework

- Considers **activation objectives** and **task-related functional connectivity**
- Models correlations in brain activity
  - **Within defined neuroanatomic regions**
  - **Between neuroanatomic regions**
- Performs global analyses (not voxel-by-voxel)
- Permits **voxel-level** and **region-level** inferences

## Limitations

- Does not account for temporal dependence **between multiple sessions**
- Fairly simple intra-regional correlation model

# Prediction Studies

- Emerging direction in neuroimaging
- Increase clinical applicability
  - Use imaging data to predict clinical outcomes (e.g. to distinguish treatment responders and non-responders)
  - We address intermediate objective of **predicting neural responses**
    - Forecast **neural representations of disease progression**
    - Predict **neural responses to various treatments**
- We develop a spatial modeling framework within this prediction context

# Motivating Data Example

- From the Alzheimer's Disease Neuroimaging Initiative (ADNI) database <http://www.loni.ucla.edu/ADNI/>.
- **Goal** of ADNI project: to develop biomarkers of Alzheimer's Disease in elderly subjects.
- Study participants receive [ $^{18}\text{F}$ ]-2-fluoro-2-deoxy-2-glucose (FDG) **PET scans** at: baseline, 6 months, 12 months and 24 months.
- In our analysis, we used the **baseline** and **month 6** scans.
- Participants classified as: mild cognitive impairment (**MCI**) patients, Alzheimer's disease (**AD**) patients, or healthy controls (**HC**).
- **Training data set**: 40 AD and 40 HC subjects; **Testing data set**: 33 AD and 33 HC subjects.



# Bayesian spatial hierarchical model

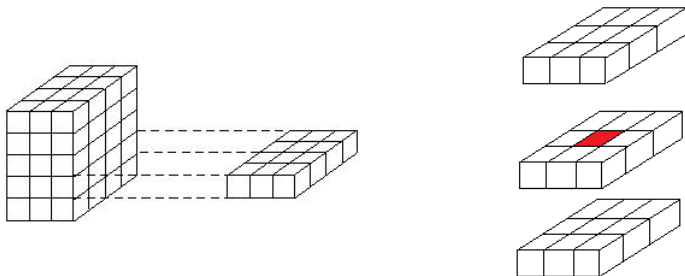
- We propose a **novel Bayesian spatial hierarchical model** for predicting follow-up neural activity based on baseline functional neuroimaging data and other patient characteristics.
- Model borrows strength from the **spatial correlations** present in the data.

## Notation

- Let  $i = 1, \dots, n$  denote subjects,  $v = 1, \dots, V$  voxels,  $g = 1, \dots, G$  regions.
- Let  $Y(v)$  denote the **regional cerebral blood flow** (rCBF) (a proxy for brain activity) at voxel  $v$ .
- Let  $\mathbf{Y}_{ig}(v) = \left( Y_{ig}(v)^{(1)}, Y_{ig}(v)^{(2)} \right)^T$ , (1)=baseline, (2)=follow-up

# Spatial dependence: 3D neighborhood

- For each voxel in the analysis, we define a **3D neighborhood** as the 26 immediate neighboring voxels.



- Borrow strength *locally*.
- We consider only within-region neighbors.
- This information is saved in a connectivity matrix  $W$ .

## Model

$$\begin{aligned}
 \mathbf{Y}_{ig}(v) | \beta_g, \phi_g, \alpha_{ig}, \gamma_{gv}, \mathbf{Z}_g &\sim N(\beta_g(v) + \phi_g(v) + \alpha_{ig} + \mathbf{X}_{ig} \gamma_g, \mathbf{Z}_g) \\
 \phi_v | \phi_{v'}, v \neq v', \Sigma, v = 1 \dots, V &\sim N\left(\rho \sum \frac{w_{v'}}{w_{v+}} \mathbf{I} \phi_{v'}, \frac{1}{w_{v+}} \Sigma\right) \quad (\text{MCAR}(\rho, \Sigma)) \\
 \beta_{gj}(v) | \lambda_{gj}^2 &\sim N(\beta_{0gj}, \lambda_{gj}^2) \quad (\lambda_{vgj} = \lambda_{gj}, \forall v \in \text{region } g) \\
 \mathbf{Z}_g^{-1} &\sim \text{Wishart}((c_1 \mathbf{\Omega}_1)^{-1}, c_1) \\
 \mathbf{\Sigma}^{-1} &\sim \text{Wishart}((c_2 \mathbf{\Omega}_2)^{-1}, c_2) \\
 \alpha_{ij} | \mathbf{\Gamma}_j &\sim N(\mathbf{0}, \mathbf{\Gamma}_j) \quad (\alpha_{ij} = \alpha_i^{(j)}) \\
 (\mathbf{\Gamma}_j)^{-1} &\sim \text{Wishart}\{(h_j H_j)^{-1}, h_j\} \quad j = 1, 2 \\
 \lambda_{gj}^{-2} &\sim \text{Gamma}(a_j, b_j) \\
 \gamma_{gjq} | \tau_{gjq}^2 &\sim N(0, \tau_{gjq}^2) \quad q = 1, \dots, Q \text{ (covariates)} \\
 \tau_{gjq}^{-2} &\sim \text{Gamma}(e_0, f_0) \\
 \rho &\sim \text{Uniform}(\{0, 0.05, 0.1, \dots, 0.9, 0.91, \dots, 0.99\})
 \end{aligned}$$

# Estimation and Prediction

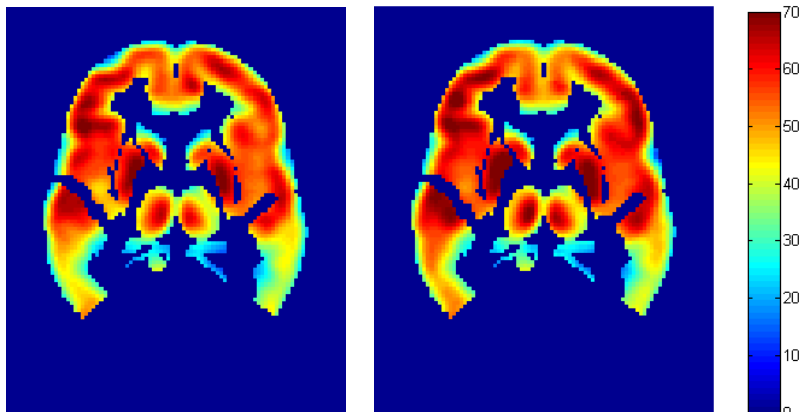
- **Estimation** is performed using MCMC techniques implemented via Gibbs sampler.
- **Prediction:**
  - For region  $g$ , we can write  $\mathbf{Y}_g = (\mathbf{Y}_{g,1}^T, \mathbf{Y}_{g,2}^T)^T \sim N((\boldsymbol{\mu}_{g,1}^T, \boldsymbol{\mu}_{g,2}^T)^T, \boldsymbol{\Sigma}_g)$ , where  $\boldsymbol{\Sigma}_g = \mathbf{Z}_g \otimes \mathbf{I}_{V_g}$ .
  - Then  $\mathbf{Y}_{i^*g,2} | \mathbf{Y}_{i^*g,1} \sim N(\mathbf{b}_{i^*g}, \mathbf{A}_{i^*g})$ , where

$$\mathbf{b}_{i^*g} = \boldsymbol{\mu}_{i^*g,2} + \boldsymbol{\Sigma}_{12}^T \boldsymbol{\Sigma}_{11}^{-1} (\mathbf{Y}_{i^*g,1} - \boldsymbol{\mu}_{i^*g,1})$$

$$\text{and } \boldsymbol{\mu}_{i^*g} = \boldsymbol{\beta}_g + \boldsymbol{\phi}_g + \mathbf{1}_{V_g} \otimes \boldsymbol{\alpha}_{i^*g} + \mathbf{1}_{V_g} \otimes \mathbf{X}_{i^*gV} \boldsymbol{\gamma}_{gV}.$$

- Inputting the posterior mean of the parameters obtained from the MCMC estimation  $\Rightarrow$  estimated conditional mean  $\hat{\mathbf{b}}_{i^*g}$
- The follow-up rCBF  $\mathbf{Y}_{g,2}$  are predicted using the mean of the estimated conditional distribution, i.e.  $\hat{\mathbf{b}}_{i^*g}$ .

# Results: Prediction for PET study of AD



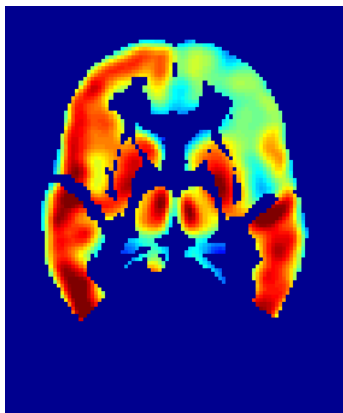
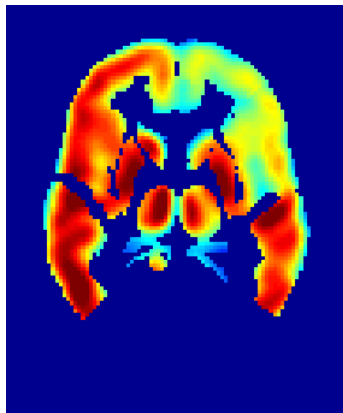
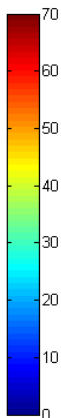
Subject 1: observed  $Y^{(2)}$

Subject 1: predicted  $Y^{(2)}$

**Figure:** Individualized observed and predicted 6 month follow-up rCBF measurements for a test subject in the AD group (axial slice 40).



## Results cont.

Subject 19: observed  $Y^{(2)}$ Subject 19: predicted  $Y^{(2)}$ 

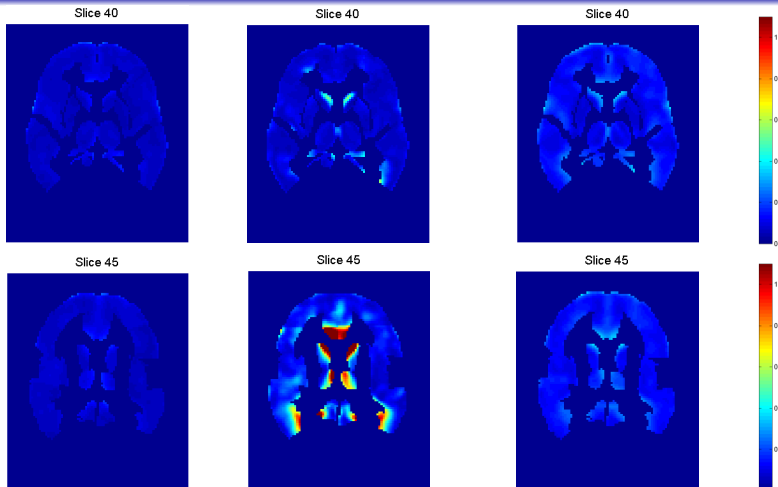
**Figure:** Individualized observed and predicted 6 month follow-up rCBF measurements for a test subject in the AD group (axial slice 40).

# Prediction Error

- We evaluate the **prediction error** using a scale-free (squared error) loss function, which adjusts for local magnitude of brain activity

$$\text{stPMSE}(\{Y_i^{(2)}(v)\}, \{\hat{Y}_i^{(2)}(v)\}) = \frac{\sqrt{\frac{1}{N} \sum_{i=1}^N [\hat{Y}_i^{(2)}(v) - Y_i^{(2)}(v)]^2}}{\frac{1}{N} \sum_{i=1}^N Y_i^{(2)}(v)}$$

# Comparative Analyses



Model

BSPM

BSMac

GLM

Aver. error

0.083

0.154 (85.5% increase)

0.157 (89.2% increase)

# Simulation Study

- We simulated 100 data sets for 15 subjects.
- Selected 5 AAL regions with sizes ranging from 234 to 4,655 voxels.
- Specified the *true* values for  $\beta_g$ ,  $\phi_g$ ,  $\alpha_i$ , and  $\gamma_g$ .
- The rest of the (hyper)parameters drawn from their prior distributions.

Param.	Region									
	1		2		3		4		5	
	True	Est.	True	Est.	True	Est.	True	Est.	True	Est.
$Z_g^{11}$	323.26	321.09	160.61	159.99	11.46	11.46	3.44	3.44	3.57	3.57
$Z_g^{22}$	120.75	120.46	45.30	45.11	37.24	37.19	10.45	10.45	3.38	3.38
$Z_g^{12}$	-41.95	-41.25	-33.70	-33.40	16.32	16.30	4.08	4.08	2.40	2.40

**Table:** Summary of the simulation results for the parameters in the covariance matrix  $\mathbf{Z}_g$ .

# Conclusions: Prediction Model

## Our model

- Incorporates both local **within-region spatial correlations** and **long-range correlations between neuroanatomic regions**.
- Accounts for **temporal dependence** between baseline and follow-up brain activity.
- Yields a method for **predicting follow-up brain activity** based on the baseline activity and relevant subject characteristics.
- Exhibits increased accuracy relative to GLM and BSMac

## Limitations

- Does not account for local spatial correlations across entire brain region
- Current estimation procedure computationally costly

# Summary

We propose:

- 1 **BSMac**: a **spatial modeling framework** for combined **activation** and **connectivity** analyses of fMRI data
  - Captures *spatial correlations*, both between voxels in the same anatomical region and between regions
  - Yields more informative analyses and more efficient estimates than conventional methods
  - Recommended use for studies in which it is not important to model correlations between multiple scanning sessions

# Summary

We propose:

- 1 **BSMac**: a **spatial modeling framework** for combined **activation** and **connectivity** analyses of fMRI data
  - Captures *spatial correlations*, both between voxels in the same anatomical region and between regions
  - Yields more informative analyses and more efficient estimates than conventional methods
  - Recommended use for studies in which it is not important to model correlations between multiple scanning sessions
- 2 A novel **prediction framework** for functional neuroimaging data
  - Captures *spatial correlations*, both between voxels in the same anatomical region and between regions, as well as *temporal correlations* between multiple scanning sessions
  - May be used for **activation** and **task-related connectivity** inferences
  - In context of prediction objectives, yields **improved prediction error**

# Acknowledgements and References

## Many thanks to

- Dr. Gordana Derado
- Dr. Ying Guo
- Dr. Lijun Zhang
- Shuo Chen

## References

- 1 Bowman, F. D. (2007). Spatio-Temporal Models for Region of Interest Analyses of Functional Neuroimaging Data. *Journal of the American Statistical Association*, 102(478), 442-453.
- 2 Bowman, F. D., Caffo, B. A, Bassett, S., and Kilts, C. (2008). Bayesian Hierarchical Framework for Spatial Modeling of fMRI Data. *NeuroImage*, 39, 1461-156.
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- 5 Guo, Y., Bowman, F.D., Kilts, C. (2008). Predicting the brain response to treatment using a Bayesian Hierarchical model with application to a study of schizophrenia. *Human Brain Mapping*, 29, 1092-1109.